

Technical aspects and safety of functional MRI

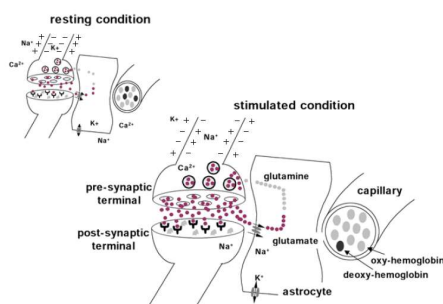
Associate Professor
Jun-Cheng Weng, Ph.D.
Chang Gung University
16 Jan 2019

Outline

- BOLD fMRI review
- Imaging method
- Imaging parameter
- Temporal resolution limitation
- Spatial resolution limitation
- Other issues
- Safety

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Physiology during neural activation



Kida and Hyder, Magnetic Resonance Imaging Methods and Biologic Applications 2006; chapter 7.

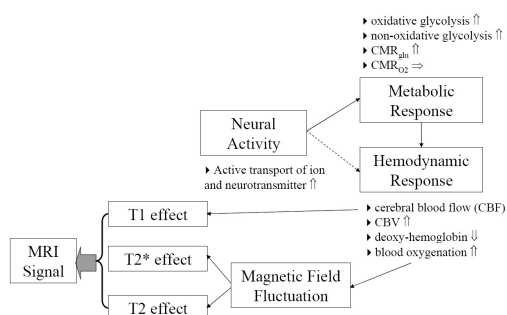
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Energy during neural activation

- **Neuronal firing: electrical activity**
 - Excitatory and inhibitory
 - Neurotransmitter release and uptake
 - Action & graded potential
 - Ion flow
 - Hormone
- **Biochemical reaction: metabolic activity**
 - Active transport of ion pumps
 - Oxidative / non-oxidative glycolysis
- **Vascular response: hemodynamic activity**
 - Energy demand, clean up waste
 - Blood flow, blood volume, blood oxygenation

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BOLD fMRI physiology



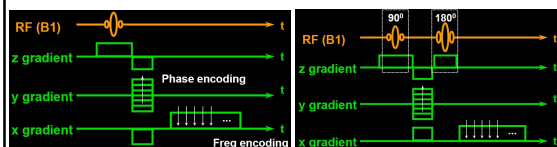
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Imaging method - contrast type

- **Gradient echo (GE) vs. spin echo (SE)**
 - Contrast: T2* vs. T2 sensitive
 - Signal: GE > SE (3-4 folds)
 - $\Delta R2^*/R2^* > \Delta R2/R2$
 - Localization: SE > GE
 - SE: micro-vasculature (capillary)
 - GE: macro-vasculature (draining vein, capillary)
 - Artifacts: GE > SE
 - susceptibility, distortion
 - Acquisition time: SE > GE

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Gradient-echo vs. spin-echo sequence



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Blood vessel effect

• Capillary

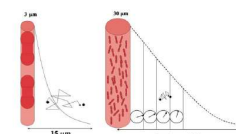
- Diffusion distance > gradient difference
- Irreversible dephasing
- T2 shorten by diffusion
- Stronger T2 effect => SE

$$S(t) = S_0 e^{-t/T_2}$$

• Large blood vessel

- Diffusion distance << gradient difference
- Reversible dephasing
- T2* shorten by average of spin
- Stronger T2* effect => GE

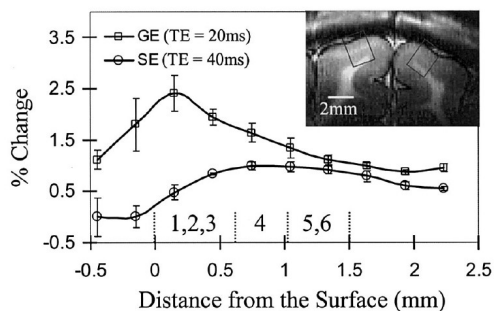
$$S(t) = \sum_j S_{0,j} e^{-t/T_2} (e^{-i\omega_j t})$$



• Kim et al., Methods 2003; 30: 28-41.

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GE vs. SE BOLD fMRI



• Zhao, et al., MRM 2004; 51: 518-524.

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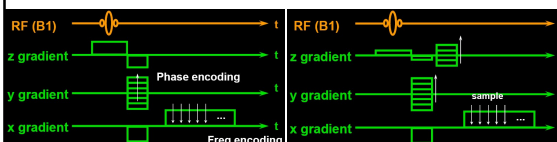
Imaging method - pulse sequence

• k-trajectory

- Fast (s per slice): FLASH / FSE
 - Higher SNR, less off-resonance artifacts
- Ultra-fast (0.1s per slice): EPI
 - Highly sensitive to T2* - > high BOLD signal
 - Subsecond resolution -> whole brain
 - Less physiological fluctuation
 - Less motion artifact
 - Less inflow artifact (infinite TR)
- 2D / 3D

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2D vs. 3D imaging pulse sequence



- 3D: Gz & Gy form two inner/outer loops

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Imaging method – 2D / 3D

• 2D multi-slice vs. 3D

	3D	2D
Benefit	<ul style="list-style-type: none"> • Rectangular slice profile • Thin slice / high resolution • Can generate arbitrary view from data • High SNR due to signal averaging of z axis (phase encoding) 	<ul style="list-style-type: none"> • Faster • Less motion artifact
Pitfall	<ul style="list-style-type: none"> • Long scan time • Motion artifact • Aliasing artifact in z 	<ul style="list-style-type: none"> • Imperfect slice profile (slice crosstalk) • Hard to get thin slice (anisotropic resolution)

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Imaging parameters

- **Important parameters:**
 - TR, TE, slice thickness, matrix size, field-of-view, bandwidth, slice order, slice gap, flip angle
- **Tradeoff among SNR, CNR, spatial/temporal resolution**
 - BOLD contrast, imaging speed, volume coverage, spatial resolution, image SNR, sensitivity to physiological activity, motion

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Tradeoff among SNR, CNR, resolution

- **TR:** temporal resolution, inflow effect, SNR, slice number
- **TE:** $\approx T2^*$
- **FA:** inflow effect
- **BW:** SNR, image acquisition time; EPI: $T2^*$ blur, distortion, chemical shift
- **FOV:** spatial resolution, SNR
- **Matrix size:** spatial resolution, SNR, imaging time
- **Slice thickness:** spatial resolution, SNR, volume coverage, partial volume
- **Slice number:** volume coverage, temporal resolution
- **Slice order/gap:** slice cross-talk

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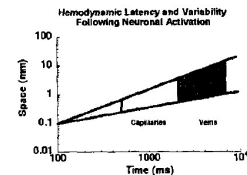
SNR and CNR

- **Signal-to-noise ratio (SNR)**
 - The most critical concern
 - Voxel size, BW, matrix, TR, FA
 - Optimal flip angle: Ernst angle $\alpha = \cos^{-1}(e^{-TR/T1})$
 - **Contrast-to-noise ratio (CNR)**
 - Voxel size: partial volume effect
 - Optimal TE = $T2^*$ of gray matter (30-40 ms @ 3T)
- $$\frac{\Delta S}{N} = \frac{S_0}{N} e^{-TE/R2^*} (TE \Delta R2^*)$$
- $$\propto \Delta R2^*/R2^* \text{ (when TE = } T2^*)$$

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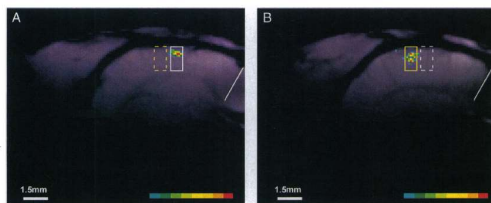
Limitations

- **Temporal**
 - The shortest neural activity
- **Spatial**
 - The accuracy of spatial localization



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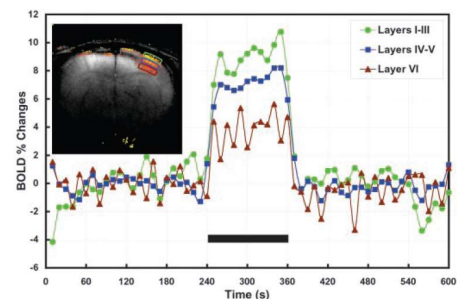
BOLD fMRI: rat whisker



- Yang, et al., PNAS 1996; 93: 473-478.

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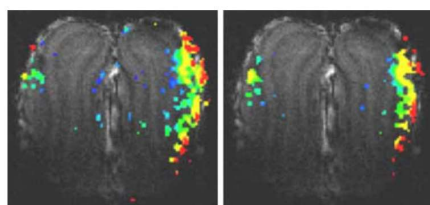
BOLD fMRI: laminar layers



- Silva and Koretsky, PNAS 2002; 99(23): 15182-15187.

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BOLD fMRI: olfactory bulb



• Xu, et al., PNAS 2003; 100: 11029-11034.

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Temporal resolution

• Physiology

- Hemodynamic response resembles a low-pass filter
- Time constant of the response function
- Limit of stimulus duration
- Detectability of difference in latency

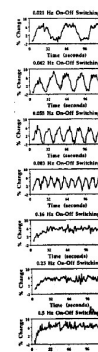
• Within one ROI

- Deconvolution of HRF
- Linear system assumption

• Across ROIs

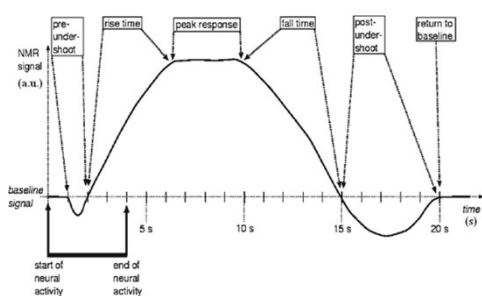
• Hardware

- Image acquisition rate: tradeoff



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Hemodynamic response function



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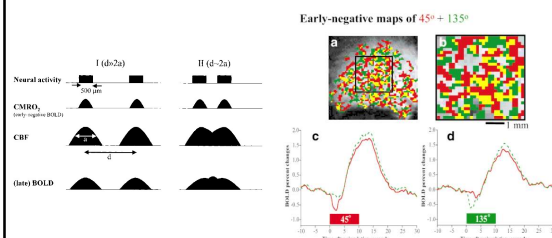
Variability of hemodynamics

• Temporal variability

- Noise
 - 1% baseline fluctuation
- HRF time constant variation
 - entire: 650ms; rise: 450ms; fall: 1250ms
- Variation over space
 - +/- 2.5s

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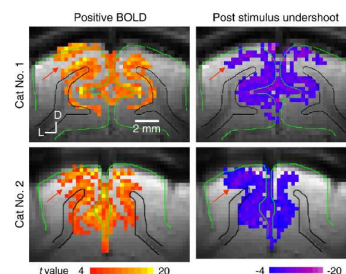
Initial dip: orientation columns in cat visual area



• Duong, et al., MRM 2000; 44:231-242

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Undershoot: cat visual cortex



• Zhao, et al., NeuroImage 2007; 34: 1084-1092.

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What's the temporal limit of

- Maximum on-off switch rate
- Minimum detectable activation duration
- Minimum detectable difference in activation duration or onset in same region
- Minimum detectable activation interval across separate brain regions
- Maximum image acquisition rate

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Current temporal limit

- Maximum on-off switch rate
 - 4 s to 8 s duration cycles
- Minimum detectable activation duration
 - 30 ms
- Minimum detectable difference in activation duration or onset in same region
 - 100 ms
- Minimum detectable activation interval across separate brain regions
 - 100 ms with normalization
- Maximum image acquisition rate
 - 64 images per sec

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Spatial resolution

- Consideration
 - CNR & SNR
 - Large vessel
 - Vessels that can not resolved by high resolution image
 - Large vein has larger signal change
 - significant at low CNR/SNR
 - Spatial limitation of hemodynamic response
 - Point spread function

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Spatial limit - CNR

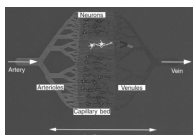
- **Signal**

$$\Delta S = \rho S_0 (e^{-TE\Delta R^2} - 1)$$
 - S_0 : control state signal
 - Proportional to voxel volume
 - ρ : active volume < 1
 - Solution: coil, higher-field
 - **Noise**
 - Random noise
 - Physiological
 - Head motion
 - System instability
- } location-dependent

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Spatial limit - macrovasculature

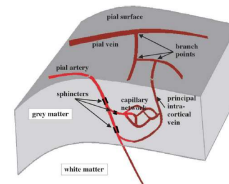
- **Inflow effect**
 - Esp for sequence using multiple excitation
 - Solution
 - Longer TR (full relaxation)
 - Shorter flip angle
 - Spin echo
- **BOLD (T2* effect)**
 - Venous T2/T2* will change during activation
 - spin-echo also affected
 - Draining/large vein effect
 - Solution
 - Bipolar gradient → suppress flowing spin in large vessels



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Spatial limit - macrovasculature

- Reduce signal from large draining vein
 - Spin-echo
 - Bipolar gradient

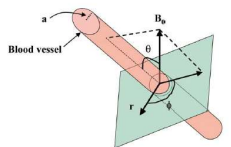


• de Zwart et al., NeuroImage 2005; 24: 667-677.

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Blood vessel effect

- Susceptibility difference: $\Delta\chi(\approx 0.27 \text{ ppm at } 37^\circ\text{C})$
- Deoxy-Hb concentration: 1-Y
- Vessel size: a
- Vessel orientation: θ, ψ
- Distance: r



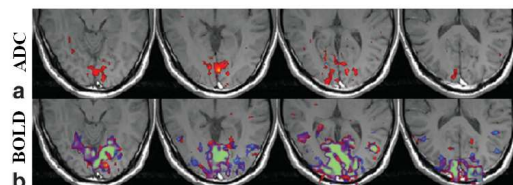
$$\Delta\omega_{\text{ax}} = 2\pi \Delta\chi_a (1 - Y) \omega_p (\cos^2\theta - 1/3)$$

$$\Delta\omega_{\text{off}} = 2\pi \Delta\chi_a (1 - Y) \omega_p (a/r)^2 (\sin^2\theta) (\cos 2\theta)$$

• Kim et al., Methods 2003; 30: 28-41.

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Biopolar gradient: human visual cortex

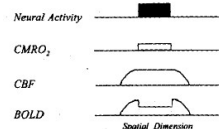


• Song, et al., MRM 2007 57: 417-422.

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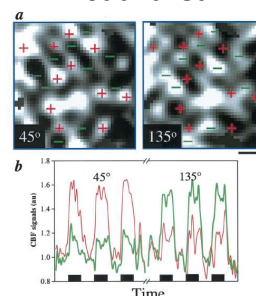
Spatial limit - hemodynamic

- Electrical activity
- Metabolic activity (closer)
 - Synaptic activity may increase in inactive neuron
- Hemodynamic activity (farther)
 - CBF
 - BOLD
 - Early negative response (closer)
 - Late positive response (farther)
- Assume CMRO₂ is exact
 - Largest signal is away



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CBF: orientation columns in cat visual area



• Duong, et al., PNAS 2001; 98: 10904-10909.

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Interpretation of fMRI signal

- fMRI signal is an index of ensemble of neural activity
 - presumably monotonic relation
- Neural source of BOLD signal is not clear
 - spiking activities vs. synaptic activity
 - excitatory vs. inhibitory
- Difficult to compare fMRI signals across cortical regions and subjects
 - BOLD signal depend on vascular structure and volume

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Other issues

- **Normal physiology condition**
 - Age
 - inferior vascular response for aged people (CBF decrease)
 - neonate: deoxyHb increase
 - Disease
 - transient global ischemia: vascular response abolished
 - carotid stenosis: vascular response diminish
 - Drug
 - alter vascular response, cardiopulmonary function,...
- **Meaning of negative response**
 - Negative response -> decreased activity?
 - Inhibitory activity also increase glucose uptake

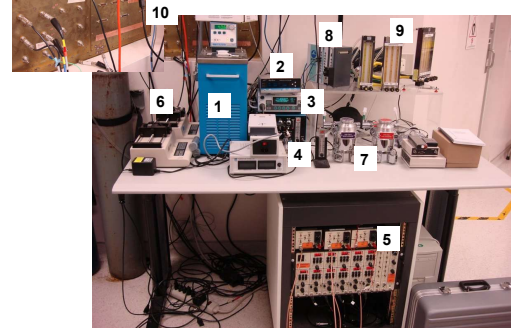
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Challenge of quantification

- **Electrical activity**
 - Tiny perturbation in magnetic field: MRI phase
 - Ca^{2+} : manganese (Mn^{2+}) enhanced MRI
 - Glutamate, GABA : ^1H -MRS
- **Metabolic activity**
 - Lactate : ^1H -MRS
 - CMRO_2 : combine CBF and BOLD
- **Hemodynamic activity**
 - Oxygenation: BOLD fMRI
 - CBF: Arterial Spin Labeling (ASL) MRI
 - CBV: contrast-injection / VASO

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fMRI equipment for animal study



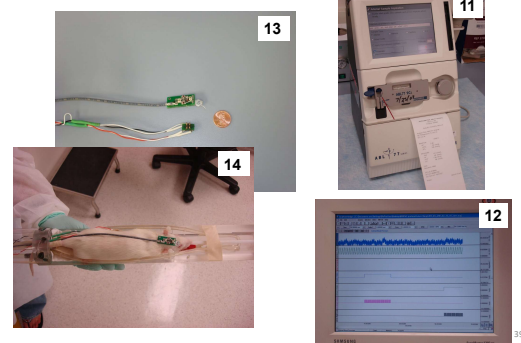
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fMRI equipment for animal study

- 1. Water bath
- 2. Temperature controller
 - temperature probe and monitor
- 3. ETCO₂ monitor
 - for monitor respiration
- 4. Ventilator
 - provide constant air flow
- 5. Electrical stimulator (4 channels)
- 6. Syringe pump
 - provide constant IV injection of anesthesia
- 7. Anesthesia
- 8. Amplifier / gating system
- 9. Air mixer
- 10. Filter panel

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fMRI equipment for animal study



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fMRI equipment for animal study

- 11. Blood gas analyzer
 - analyze blood pH, pO_2 , and pCO_2
 - maintain the same BOLD condition
- 12. Physiological monitoring, gating software
 - record arterial blood pressure, rectal temperature, ETCO₂, EPI trigger
 - output trigger pulse to stimulator and/or MRI
- 13. Coil, electrode
- 14. Rat holder positioning stand (in MRI)
 - with ear bar and bite bar

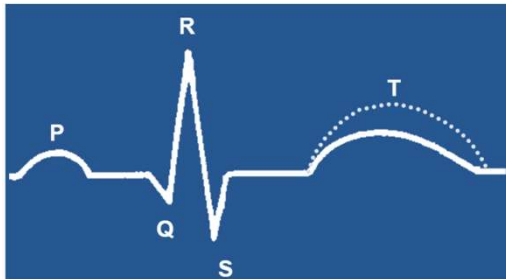
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Bioeffects of Main Field

- Enhanced T-wave in ECG
- Magnetohydrodynamic effect
- Blood is electrically conductive
- Electrical induction from moving conductor in magnetic field
- Detected by ECG surface electrodes

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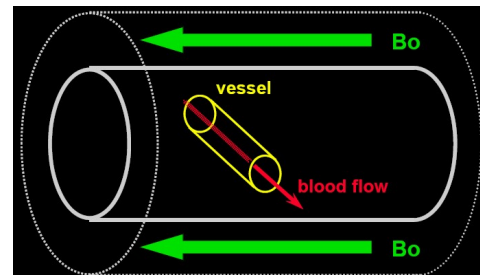
Enhanced T-wave in Electrocardiogram



- A known effect from MRI main field

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Magnetohydrodynamic Effect



- Electrical induction from moving conductor

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RF Bioeffects

- Local temperature increases with too much RF
- FDA: specific absorption rate (SAR) limits (2004):
 - Mean < 3.0 W/Kg in head
 - Mean < 4.0 W/Kg whole-body
 - Mean < 8.0 W/Kg body (軀幹)
 - Mean < 12 W/Kg locally (四肢)
- Automatic detection by MRI system (body weight)
- Related to protocol, e.g. fast spin echo

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Heating Effects from RF

- Temperature raise induced by RF
 - ~1°C
 - Head < 38°C, body < 39°C, limbs < 40°C
- Homeostasis for maintaining body temperature in human
- Blood flow carries away the heat

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Gradient Bioeffects

- Magnetophosphene
- Rapid B_0 change on conductive human body
- Electric induction due to fast dB/dt
- Flash-like vision when optic nerves fire action potential

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Magnetophosphene

- Smaller effects near MRI isocenter
- Peripheral nerve stimulation
- Response gone after scan stops
- Optic nerves unharmed
- Present in EPI scan only

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Protection for MRI Safety

- What kind of protection do we need if MRI is so safe?
- No worry under normal operation
- Abnormal operation can be extremely dangerous

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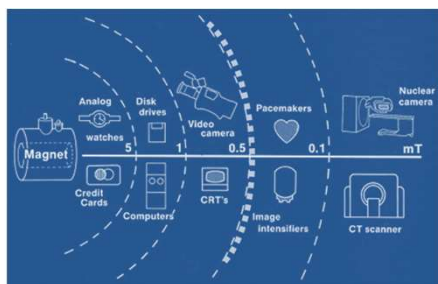
The Strong MRI Magnet

- Earth field: 0.5 Gauss
- Toy magnets: ~ 50 Gauss
- MRI magnet: 15,000~117,000 Gauss



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Magnetic Effect to Electronic Devices



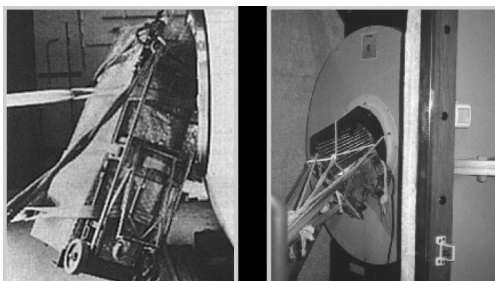
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Danger of Strong B_0

- Huge attractive force for appliance
 - Nail scissors, tweezers
 - Wrench, screwdriver, hammer
 - Computer, chair, oscilloscope

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Danger of Ferromagnetic Object in MRI



Power amplifier

De-humidifier

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Danger of Ferromagnetic Object in MRI

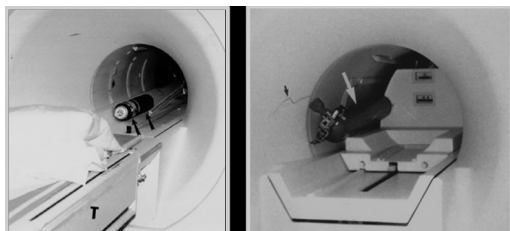


Chair

Buffer

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Danger of Ferromagnetic Object in MRI



Nitrous oxide tank

Oxygen cylinder

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Danger of Ferromagnetic Object in MRI



Vacuum cleaner

i.v. injector

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Other “Bad” Things

- Metal or magnetic stuff
 - Implants
 - Surgical clips
 - Cochlear implants
 - Injection pump
 - Prosthesis
 - Carry-on
 - Dental work
 - Leather belt
 - Make-up (eye shadow)
 - Hair pin
- Discomfort or image distortions

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Some Known “Bad Things”



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Superfunction or Susceptibility Artifact



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Safety information



- http://www.mrisafety.com/safety_info.asp

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Thank you for your attention

May the force be with you